

# A fast full multigrid solver for applications in image processing

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# Motivation

## Challenges of Medical Image Processing

- large volume data sets ( $512^3$  voxels and more)

or / and

- real time performance

## Variational Approaches

typically elliptic PDE

- e. g. image denoising
- e. g. non-rigid image registration

- optimized MG solver for time-dependent Poisson equation
- compare with optimized FFT-based implementations

# Contents

- 1 Introduction
  - Motivation
  - Model Problem
- 2 A hardware-optimized MG solver
  - SIMDization and blocking
  - Runtime MG vs. FFT
  - MG convergence rates
- 3 Applications
  - Image denoising by blurring
  - Non-rigid medical image registration

# Linear Heat Equation

$$\frac{\partial u}{\partial t}(\mathbf{x}, t) - \Delta u(\mathbf{x}, t) = f(\mathbf{x}), \quad u(\mathbf{x}, 0) = u_0(\mathbf{x}) \quad (1)$$

with time  $t \in \mathbb{R}^+$ ,  $u, f : \Omega \subset \mathbb{R}^3 \rightarrow \mathbb{R}$ ,  $\mathbf{x} \in \Omega$ ,  
initial solution  $u_0 : \Omega \subset \mathbb{R}^3 \rightarrow \mathbb{R}$  and  
homogeneous Neumann boundary conditions.

(1) is discretized using finite differences

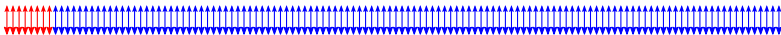
$$\frac{u_h(\mathbf{x}, \tau) - u_0(\mathbf{x})}{\tau} - \Delta_h u_h(\mathbf{x}, \tau) = f_h(\mathbf{x}), \quad (2)$$

on a regular grid  $\Omega_h$  with mesh size  $h$  and time step  $\tau$ .

Cell-based multigrid solver using averaging restriction,  $\omega$ RBGS  
smoother and constant interpolation.

# Single Instruction Multiple Data

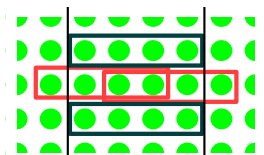
- Buses become wider and wider but ineffective for scalar operations.



- SIMD units exploit the wider buses if
  - the same operation is done on neighboring values

$$\begin{bmatrix} a_0 \\ a_1 \\ a_2 \\ a_3 \end{bmatrix} * \begin{bmatrix} b_0 \\ b_1 \\ b_2 \\ b_3 \end{bmatrix}$$

- and data is naturally aligned in memory.
- Example: SIMDized 2D Poisson Jacobi



SIMDized  $\omega$ RBGS

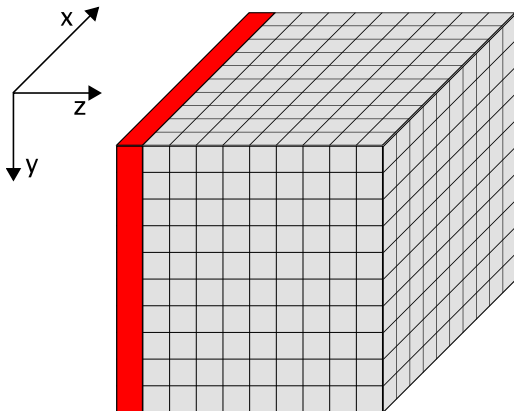
Using two – per line – constant SIMD registers, we can treat vector members differently:

$$\begin{bmatrix} u_a^{\text{new}} \\ u_b^{\text{new}} \\ u_c^{\text{new}} \\ u_d^{\text{new}} \end{bmatrix} = \begin{bmatrix} 1 - \omega \\ 1 \\ 1 - \omega \\ 1 \end{bmatrix} * \begin{bmatrix} u_a^{\text{old}} \\ u_b^{\text{old}} \\ u_c^{\text{old}} \\ u_d^{\text{old}} \end{bmatrix} + \begin{bmatrix} \omega \\ 0 \\ \omega \\ 0 \end{bmatrix} * \begin{bmatrix} u_a^{\text{jac}} \\ u_b^{\text{jac}} \\ u_c^{\text{jac}} \\ u_d^{\text{jac}} \end{bmatrix} .$$

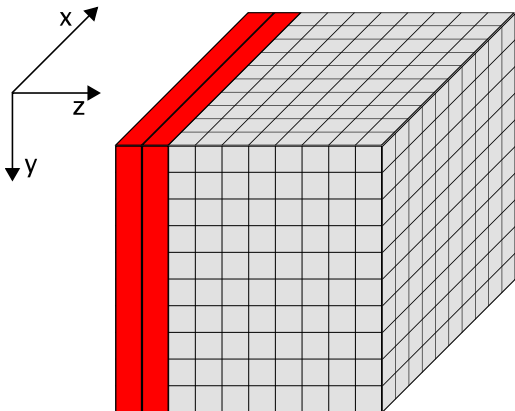
A red or black  $\omega$ RBGS sweep is computationally about as expensive as a damped Jacobi.

Although we effectively invalidate half FLOPs done, the better internal and external bandwidth of SIMD over the scalar unit leads to a real performance gain.

# Simple Plane Blocking

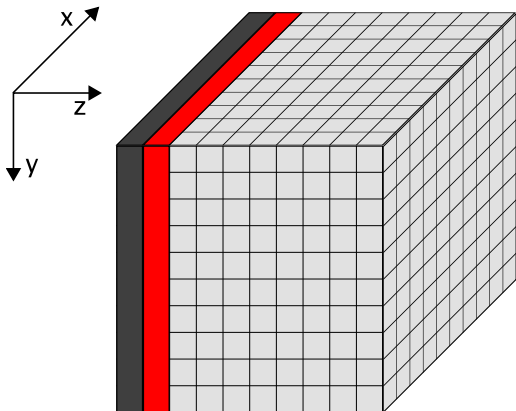


# Simple Plane Blocking

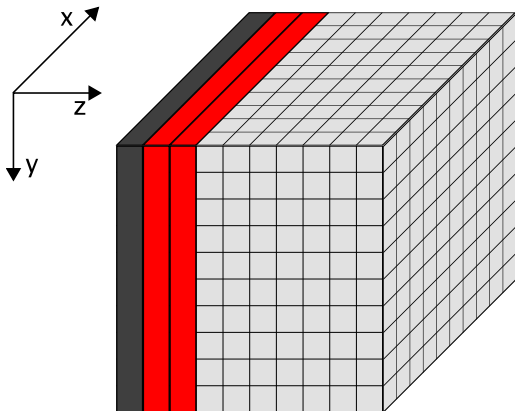




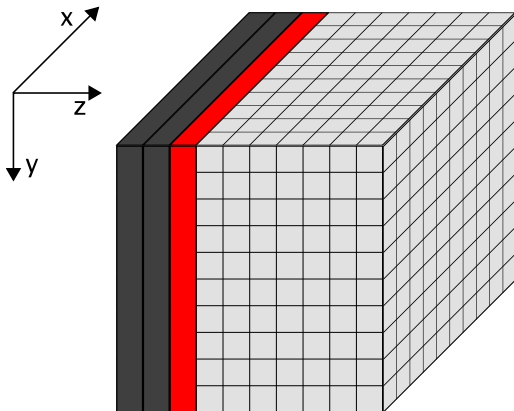
# Simple Plane Blocking



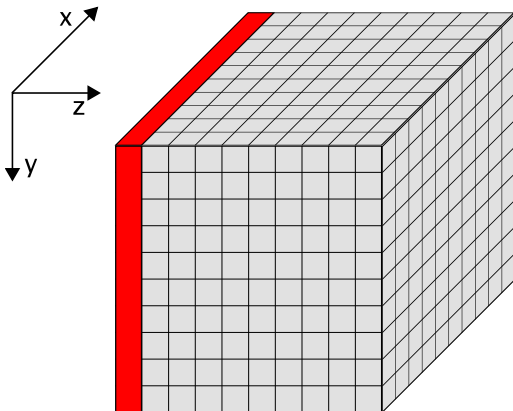
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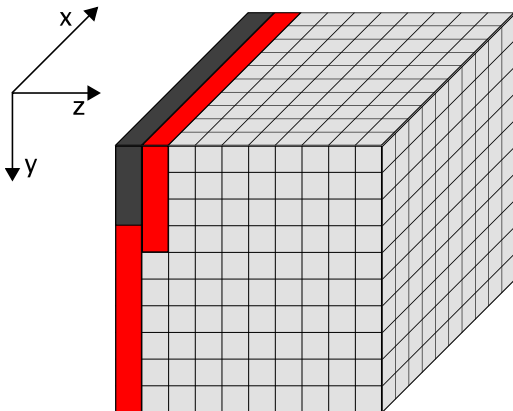
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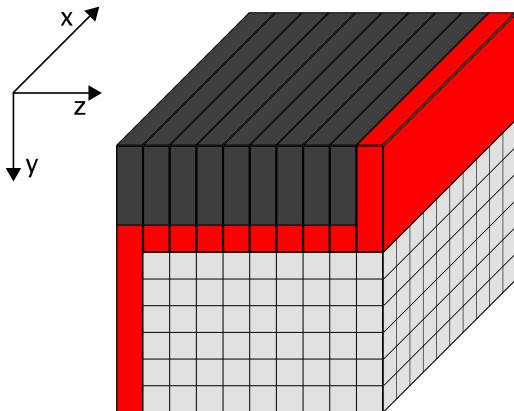
# Sub-Blocking



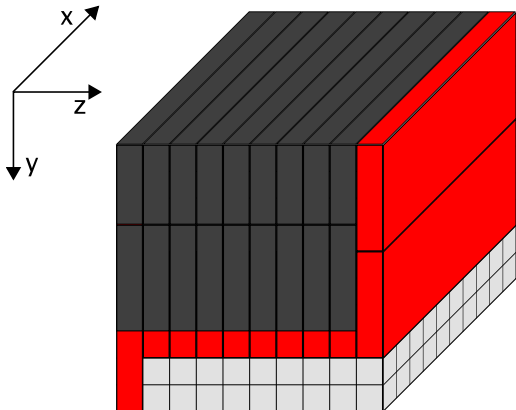
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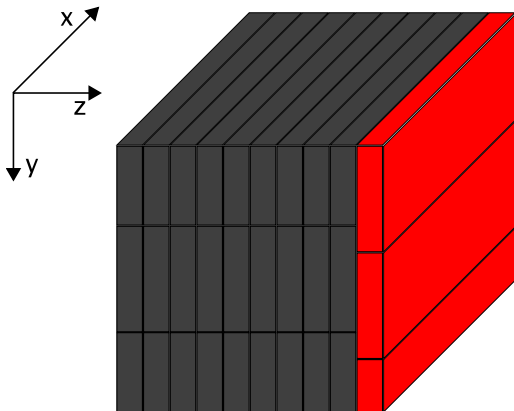
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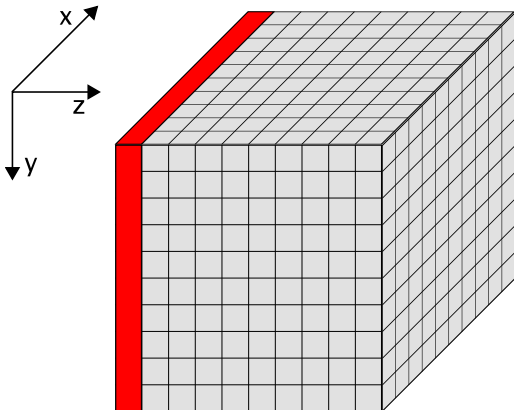


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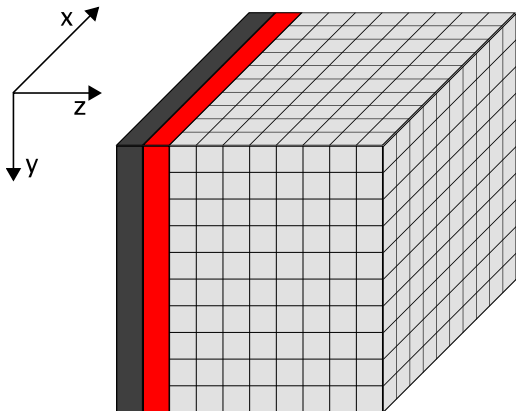




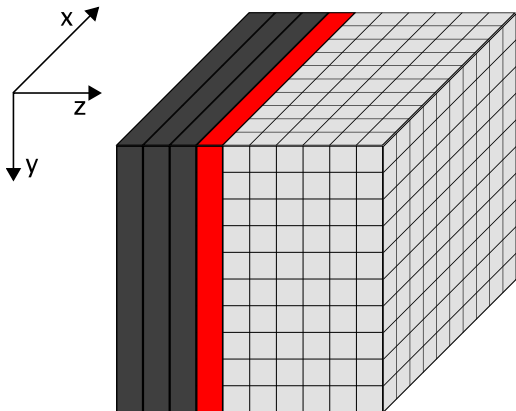
# Fusion with Calculation of Residual and Restriction



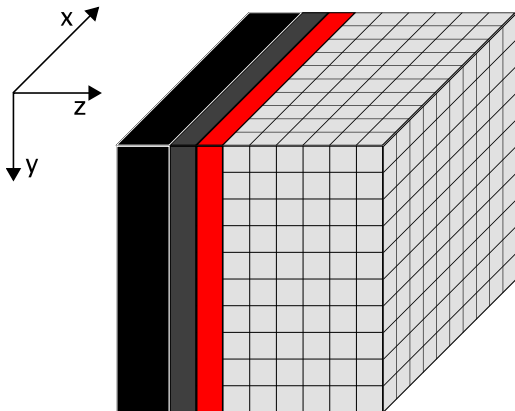
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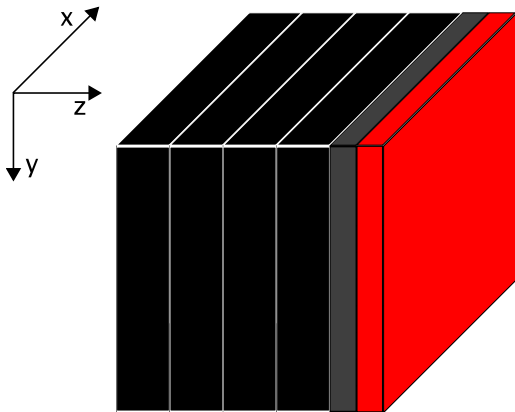
# Fusion with Calculation of Residual and Restriction



# Fusion with Calculation of Residual and Restriction



# Fusion with Calculation of Residual and Restriction



## MG vs. FFT

	V	FMG	FMG	FFT	DCT	FFT
size	(1,1)	V(1,1)	V(2,2)	(fftw)	(fftw)	(mkl)
32	0.43	0.55	0.93	0.40	1.43	0.71

**Table:** Wallclock times in ms for FFT (real type, out of place, forward and backward) and the optimized multigrid on an Intel Core2 Duo 2.4 GHz (Conroe) workstation.

## MG vs. FFT

size	V (1,1)	FMG V(1,1)	FMG V(2,2)	FFT (fftw)	DCT (fftw)	FFT (mkl)
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64	3.33	4.29	7.12	3.73	12.2	5.27

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128	31.6	44.1	68.3	50.4	123	45.8

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256	264	370	574	473	1246	401

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256	264	370	574	473	1246	401
512	2168	3026	4699	4174	11067	3510

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# Convergence Rates

size	$\tau$	V(1,1)	V(2,2)
$64^3$	$10^4$	0.26	0.07
$128^3$	$10^4$	0.28	0.07
$256^3$	$10^4$	0.29	0.07
$512^3$	$10^4$	0.32	0.07
$64^3$	$10^{30}$	0.27	0.07
$128^3$	$10^{30}$	0.29	0.07
$256^3$	$10^{30}$	0.32	0.07
$512^3$	$10^{30}$	0.34	0.07

**Table:** Convergence rates measured experimentally for  $h = 1.0$  on the finest grid and 1 grid point on the coarsest level using 100 vector iterations (power method).

# Image Denoising: Model

Simple variational based on Tikhonov regularization, minimizing the functional

$$E_1(u) = \int_{\Omega} |u_0 - u|^2 + \alpha |\nabla u|^2 d\mathbf{x} \quad (3)$$

with  $\mathbf{x} \in \mathbb{R}^d$  and  $\alpha \in \mathbb{R}^+$  over image domain  $\Omega \subset \mathbb{R}^d$ .

Necessary condition for a minimizer  $u$  (the denoised image) is characterized by the Euler-Lagrange equation

$$u - u_0 - \alpha \Delta u = 0 \quad (4)$$

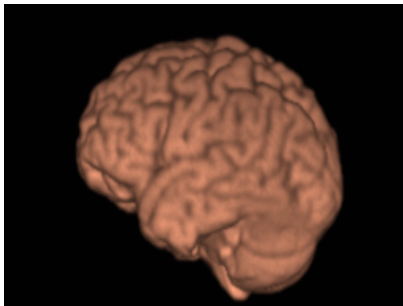
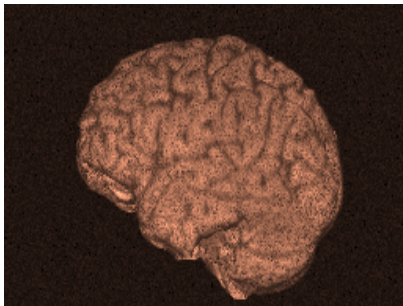
with homogeneous Neumann boundary conditions.

## Image Denoising: Computation

- 1 Convolution of the image with a discrete version of the Gaussian kernel (stencil),
- 2 multiplication in Fourier space (5) or

$$F[G_\sigma * u_0](\mathbf{w}) = e^{-|\mathbf{x}|^2/(2/\sigma^2)} F[u_0](\mathbf{w}) \quad (5)$$

- 3 application of a multigrid method to (2).



# Image Denoising: Runtimes

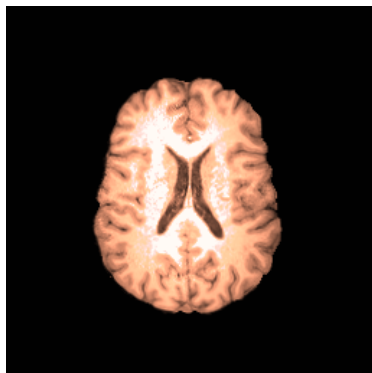
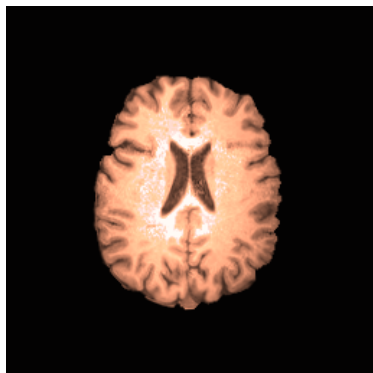
method	runtime
filtering with mask of size $5 \times 5 \times 5$	1200 ms
filtering with mask of size $3 \times 3 \times 3$	681 ms
$V(1, 1)$ -cycle	390 ms
FFTW-package	1140 ms

**Table:** Runtime for image denoising using a 3D MRI image (size  $256 \times 256 \times 160$ ) of a human head with added Gaussian noise, measured on the AMD Opteron platform.

# Image Registration: Model I

Variational approach to minimize the energy functional

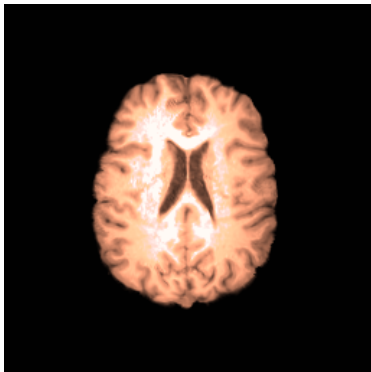
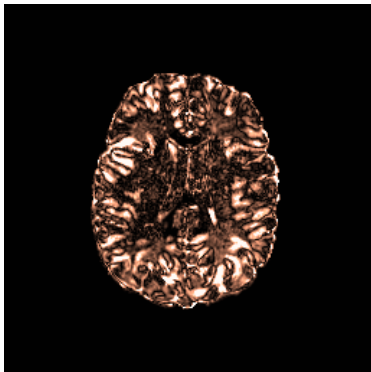
$$E_2(u) = \int_{\Omega} (T(\mathbf{x} - \mathbf{u}(\mathbf{x})) - R(\mathbf{x}))^2 + \alpha \sum_{l=1}^d \|\nabla u_l\|^2 d\mathbf{x} . \quad (6)$$



# Image Registration: Model II

The optimization of the energy functional results in nonlinear Euler Lagrange equations. To treat the nonlinearity, an artificial time is introduced and discretized by an semi-implicit scheme:

$$\frac{(\mathbf{u}_h^{k+1} - \mathbf{u}_h^k)}{\tau} - \alpha \Delta_h \mathbf{u}_h^{k+1} = \nabla_h T(\mathbf{x} - \mathbf{u}_h^k) (T(\mathbf{x} - \mathbf{u}_h^k) - R(\mathbf{x})) \quad (7)$$





# Image Registration: Runtimes

method	runtime
FMG-V(2,2)	608 ms
FMG-V(2,1)	499 ms
FMG-V(1,1)	390 ms
DCT	2107 ms
AOS	1971 ms

**Table:** Runtime for one linear solve in one time step in the image registration algorithm for an image of size  $256 \times 256 \times 160$ .

## Future Work

- Extend multigrid solver to (an)isotropic diffusion.
- Implement on CBEA.



## Convergence Rates According to LFA

interpolation	$\omega$	V(1,1)			V(2,2)		
		$\rho$	$\rho(M_{3L})$	$c_{exp}$	$\rho$	$\rho(M_{3L})$	$c_{exp}$
constant	1.0	0.20	0.47		0.04	0.07	
constant	1.15	0.08	0.20	0.27	0.04	0.06	0.07
trilinear	1.15	0.08	0.10		0.04	0.06	

**Table:** Smoothing factor ( $\rho$ ) and three-grid asymptotic convergence factor ( $\rho(M_{3L})$ ) for size  $64^3$ ,  $\tau = 10^{30}$  obtained by LFA (using the `lfa` package from R. WIENANDS).

# Image Denoising: Gaussian Kernel

In an infinite domain an explicit solution is given by

$$u(\mathbf{x}, t) = \int_{\mathbb{R}^d} G_{\sqrt{2t}}(\mathbf{x} - \mathbf{y}) u_0(\mathbf{y}) d\mathbf{y} = (G_{\sqrt{2t}} * u_0)(\mathbf{x}) , \quad (8)$$

where the operator  $*$  denotes the convolution of the grid function  $u_0$  and the Gaussian kernel

$$G_\sigma(\mathbf{x}) = \frac{1}{2\pi\sigma^2} e^{-|\mathbf{x}|^2/(2\sigma^2)} , \quad (9)$$

with standard deviation  $\sigma \in \mathbb{R}^+$ . This is equivalent to applying a low-pass filter and can be transformed into Fourier space, where a convolution corresponds to a multiplication of the transformed signals.

# Image Denoising: FFT

If we denote by  $F[f]$  the Fourier transform of a signal  $f : \mathbb{R}^d \rightarrow \mathbb{R}$  and use

$$F[G_\sigma](\mathbf{w}) = e^{-|\mathbf{x}|^2/(2/\sigma^2)}, \mathbf{w} \in \mathbb{R}^d$$

it follows that

$$F[G_\sigma * u_0](\mathbf{w}) = e^{-|\mathbf{x}|^2/(2/\sigma^2)} F[u_0](\mathbf{w}) . \quad (10)$$

# Image Registration: Functional

The optimization of the energy functional results in nonlinear Euler Lagrange equations

$$\nabla T(\mathbf{x} - \mathbf{u}(\mathbf{x})) (T(\mathbf{x} - \mathbf{u}(\mathbf{x})) - R(\mathbf{x})) + \alpha \Delta \mathbf{u} = 0 \quad (11)$$

with homogeneous Neumann boundary conditions that can be discretized by finite differences on a regular grid  $\Omega_h$  with mesh size  $h$ . To treat the nonlinearity often an artificial time is introduced

$$\partial_t \mathbf{u}(\mathbf{x}, t) - \alpha \Delta \mathbf{u}(\mathbf{x}, t) = \nabla T(\mathbf{x} - \mathbf{u}(\mathbf{x}, t)) (T(\mathbf{x} - \mathbf{u}(\mathbf{x}, t)) - R(\mathbf{x})) \quad (12)$$

that is discretized by a semi-implicit scheme with a discrete time step  $\tau$ , where the nonlinear term is evaluated at the old time level

$$\frac{(\mathbf{u}_h^{k+1} - \mathbf{u}_h^k)}{\tau} - \alpha \Delta_h \mathbf{u}_h^{k+1} = \nabla_h T(\mathbf{x} - \mathbf{u}_h^k) \left( T(\mathbf{x} - \mathbf{u}_h^k) - R(\mathbf{x}) \right). \quad (13)$$